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Expandable intraluminal endoprosthesis.

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5 The present invention relates to an expandable intraluminal endoprosthesis comprising a tubular member having a first and second end and a wall surface disposed between said first and second end, the wall having a substantially uniform thickness and having a first diameter in a first, unexpanded state which permits intraluminal delivery of the member into a lumen of a body passageway, particularly a blood vessel, which member is capable of acquiring a second diameter in an expanded and deformed state upon the application from the interior of the tubular member of a radially outwardly extending force, which second diameter is variable and dependent on the amount of said force applied to the tubular member, whereby the tubular member may be expanded and deformed to expand the lumen of the body passageway. More particularly the invention relates to an expandable intraluminal vascular endoprosthesis which is especially useful for repairing or reconstructing blood vessels narrowed or occluded by a disease.

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15 Commonly this kind of medical device is referred to as vascular stent or graft.

Stents are prosthetic devices which are implanted inside a lumen in order to provide support for its wall and to assure an undisturbed flow through the lumen. This is particularly important in the field of angioplasty which is concerned with the repair and reconstruction of blood vessels. In that particular field stents are implanted within the vascular system to reinforce collapsing, partially occluded, weakened, or abnormally dilated sections of blood vessels. More generally, however, stents can be used inside the lumen of any physiological conduit or duct including the arterics, veins, bile ducts, the urinary tract, alimentary tracts, the tracheobronchial tree, a cerebral aqueduct and the genitourinary system. Moreover stents can be used inside lumina of animals besides humans.

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Generally two types of stents may be distinguished. First there are self-expandable stents which automatically expand once they are released to assume a permanent deployed, expanded state. These stents expand to a defined diameter and are unable to remodel the true vascular anatomy over lengths greater than 2 cm. Their drawback is that the physician needs to place the right device and thereby has to rely on information derived from fluoro and angiographic equipment. A second type of stents concerns the

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so-called balloon expandable stents which generally involve a tubular member capable of receiving a balloon of a balloon-tipped catheter by means of which it may be deployed. The present invention particularly pertains to this second kind of stents.

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A common procedure for implanting a balloon-expandable stent in a blood vessel involves mounting the stent in its unexpanded, crimped state on a balloon-tip catheter of a suitable delivery system. The catheter is then slipped through an incision in the vessel wall and down the length of the vessel until it is positioned to bridge the diseased or narrowed portion of the vessel. The stent is then expanded with the aid of the balloon-catheter against the internal wall of the vessel. This may be done after the vessel has been predilated and it has been determined that a stent is necessary. Alternatively the vessel could be dilated by the stent itself while the latter is expanded by means of the balloon. *In* both cases the stent will maintain its deployed, expanded form once the balloon is evacuated and the catheter retracted again in order to provide a permanent support for the blood vessel concerned.

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A wide overview of vascular stents which are nowadays available is given in the Handbook of Coronary Stents by Patrick W. Serruys et al. of the Rotterdam Thoraxcentre Interventional Cardiology Group. This overview describes at page 21 ff. the so called Palmaz-Schatz™ stent as the gold standard in the field of stents. This stent concerns a number of consecutive slotted tubes of stainless steel which are mutually connected by means of one or more bridges. Although this stent is most widely used and tested in practice, it has been implanted in over 600000 patients all over the world, it still suffers from a number of drawbacks. The main drawbacks have to do with the stent-to-vessel-ratio uniformity and crimped as well as deployed flexibility. The stent-to-vessel-ratio involves the degree to which the vessel is supported by the stent in its expanded state and should not only be high, but preferably also uniform throughout the length of the stent. However, due to the inevitable bridges between adjacent tubes of the Palmaz-Schatz™ stent, there will be a bare area between adjacent segments of the stent once it has been deployed giving rise to a decreased and even poor stent-to-vessel-ratio at these locations. The other drawback concerns the rather high rigidity of the stent

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segments in their crimped and deployed state. As a consequence the stent has only a limited flexibility which hinders the delivery of the stent to its intended position inside the body. The poor deployed flexibility of this stent gives rise to a straightening of the vessel over segments longer than typically 2 cm which appears to be a primary cause for late term restenosis of the stented area. Typically this occurs after about 6 months after surgical post procedural.

A balloon expandable stent with a highly uniform stent-to-vessel ratio as well as an excellent flexibility in its crimped state is described at page 63 ff. of the same reference and concerns the Cordis Coronary Stent. This device is composed of a single piece of tantalum (Ta) wire. The wire is wrapped to form a continuous sine wave and helically wound along a longitudinal axis. Both ends of the wire are weld terminated. A similar device was presented at the annual symposium of the Radiological Society of North America (RSNA) 11/95. This peripheral stent embodiment incorporates intermediate welds, patterned through the length of the stent. This device contains adjacent helical turns of the wire which are welded together at adjoining locations and exhibits a highly regular distribution of the wire along the length of the device. Its properties, such as crimped profile and stent-to-vessel ratio, are uniform over its length both in the crimped and deployed states. However, because of its constitution this device offers only a poor design freedom when it comes to tailoring the design to add specific functionality and remove certain drawbacks. Also the internal stress in the device once it has been wound hinders the provision of reliable welds between adjacent turns. These welds as well as those to the ends of the wire moreover remain a weak point especially during expansion of the device.

It is an aim of the present invention to provide a balloon expandable stent which combines a high degree of uniformity and flexibility with excellent design capabilities.

To this end an expandable intraluminal endoprosthesis of the kind described in the opening paragraph according to the invention is characterized in that at least in said first unexpanded state at least a part of said wall of said tubular member comprises a

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substantially continuous structure of mutually staggered undulations which has been separated from a tube wall, in that said substantially continuous structure comprises at least one pattern which advances substantially helically along a longitudinal axis of said tubular body and in that said structure comprises connection elements connecting adjacent undulations, which connection elements are an integral extension of the undulations which they connected.

The structure making up the wall of the tubular member may be separated from a hollow tube by means of for instance laser cutting or a similar technique available to a skilled person. In this manner a substantially stress-free structure may be created incorporating a substantially helically advancing pattern which can be highly uniform and flexible throughout the length of the device but still facilitates unimpaired design freedom to tailor the pattern to meet additional functionality and to remove specific drawbacks. Moreover as the connecting elements are likewise separated from the tube as the rest of the structure and consequently are entirely integral with said structure the drawbacks associated with the welds in the prior art device may be avoided. The substantial helical pattern within the structure may be designed to form, upon deployment, a substantially continuously advancing spine as a kind of backbone of the device.

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C3) A specific embodiment of the endoprosthesis according to the invention is characterized in that said structure comprises a continuous filament which is separated from a tube wall, in that said adjacent undulations are staggered in a substantially helical configuration advancing along a longitudinal axis of the tubular body to form one of said at least one substantially helical pattern within said structure, and in that a first helical turn of said filament around said longitudinal axis of said tubular member is connected to an adjacent second such turn of said filament by means of at least one of said connection elements, being an integral extension of said filament. This embodiment to large extent compares to the Cordis Coronary Stent referred to above, without however sharing the above described drawbacks of that device.

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In order to improve on flexibility in a compressed as well as in a deployed state of the device a further specific embodiment of the endoprosthesis is according to the invention characterized in that adjacent turns of said filament are connected to one another by means of a number of connection elements less than the number of undulations in said turns. Due to the fairly unlimited design freedom in the device of the invention, the number of interconnections between adjacent turns may be adapted freely to suit the flexibility of the device. The less connection between adjacent turns, the more flexible the device will be. Said design freedom moreover allows a variation of the number of interconnections between adjacent turns within the same device to suit an optimal behaviour.

In a preferred embodiment an endoprosthesis is according to the invention characterized in that said structure comprises a number of turns of said filament whereby the connection elements to subsequent turns are radially shifted to form at least one further substantially helical pattern of said at least one substantial helical pattern within said structure. In this manner a kind of primary framework structure may be obtained which supports the vessel wall while maintaining deployed flexibility. More specifically a preferred embodiment of the endoprostehesis according to the invention is chracterized in that at least a portion of the structure comprises a number of connection elements which are substantially equally divided in each turn of said filament and in that connection elements in successive turns are helically shifted by approximately one undulation pitch distance. By shifting the connection elements substantially a full pitch distance a structure is realized in which successive connection elements are linked to each other by substantially a full undulation of said first pattern. This undulation introduces significant slack and expandable diameter within the helical spine created by the interlinked connection elements which allows a very gradual expansion of the device tranverse to its longitudinal direction. This reduces so called foreshortening which is a longitudinal shrinking of the device as it is expanded and would otherwise limit the effective range of the device.

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A further specific embodiment of the device according to the invention is characterized in that at least some of the connection elements comprise a strut diagonally interconnecting a first side of a first adjoining undulation to an opposite side of a second adjoining undulation, the strut being entirely integral with said adjoining undulations and having a direction different to the helical direction of said one substantial helical pattern within said structure. Upon deployment, this structure will create a kind of spine which runs over a series of connection elements in a different, or even contra-, helical direction compared to that of said one substantially helical pattern. Such multiple-helix structure is capable of withstanding a significant hoop strength whilst still being flexible and conformal to the natural vessel wall.

In a still further embodiment an endoprosthesis is according to the invention characterized in that the connection elements to subsequent turns are radially shifted by approximately one undulation pitch distance. Due to this regular pattern of connection elements one or more continuous, helically turning spines will be obtained in the deployed state of the device, formed by subsequent struts and the respective sides of the undulations they interconnect. These spines may form a scaffolding lattice which uniformly supports the vessel wall while maintaining deployed flexibility in order to be as conformal as possible with the natural form of the vessel concerned. It has been found that especially lack of the latter, resulting in <sup>an</sup> unnatural straightening of the vessel over a certain length, is a primary cause for late term restenosis of the stented segment. Due to the deployed flexibility and its highly conformal deployed shape this still further embodiment of the invention aims to avoid this problem.

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To further improve on flexibility while maintaining hoop strength, i.e. the ability to withstand inwardly directed radial forces, a further specific embodiment of the endoprosthesis according to the invention is characterized in that the first side of said first undulation, said opposite side of said second undulation and said strut have a first filament width and in that the opposite side of said first undulation and the first side of the second undulation have a second filament width, the first filament width being larger than the second filament width. The inventor has recognized that said second

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filament width may be made smaller than said first filament width, thus gaining flexibility, without deteriorating the strength of the device and particularly its radial hoop strength.

5 In a further specific embodiment the endoprosthesis according to the invention is characterized in that said strut connecting opposite sides of adjoining undulations of subsequent turns have a substantially S-shaped structure. Such a double curved structure of the connection elements creates more slack between mutually interconnected undulations allowing more expansion as well as an improved stent to vessel ratio at said  
10 area once the prosthesis has been deployed.

A still further preferred embodiment of the endoprosthesis according to the invention is characterized in that the connection elements each comprise two intersecting struts which are entirely integral with each other and with the adjoining undulations which  
15 they connect. The inventor has recognized that on deployment of the device such an interconnection element will first rotate around its central axis before the entire force applied pulls axially on the point of intersection. As a consequence a certain stress relief is incorporated in the device which allows for a smaller filament width. This does not only add to the flexibility of the device but also leads to a more favourable radio-  
20 opacity. Moreover, the intersecting struts leave a substantially unchanged scaffolding area or footprint upon deployment of the structure thereby improving on the eventual stent-to-vessel ratio of the device compared to a connection element which will almost entirely stretch upon deployment.

25 The design freedom gained by the endoprosthesis according to the invention appears fairly unlimited and can be applied to precisely tailor the properties of the device to specific requirements. Not only the form, number and the location of connection elements but also the filament width and form of particular parts may be adapted in this sense. As an example, a further specific embodiment of the invention is characterized in  
30 that the undulations in said filament have a first mutual pitch in a first of said turns of said filament and a second mutual pitch in a second of said turns, the first and second

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pitch being different from each other. Varying the mutual pitch of the undulations will generally give rise to more or less flexibility in combination with less or more vessel support at the zones concerned.

5 A still further embodiment of the endoprosthesis according to the invention is characterized in that at least a part of at least one undulation in at least one turn of said at least one substantially helical pattern has an increased amplitude, while at least the adjoining part of an adjoining undulation in an adjacent turn has a correspondingly decreased amplitude. In this case the mechanical properties of the device and especially  
10 the manner of deployment as well as the stent-to-vessel ratio may be tailored by offsetting the point where adjacent undulations meet.

More specifically a further embodiment of the endoprosthesis according to the invention is characterized in that a first pair of adjacent undulations of said structure is connected  
15 by means of a first connection element, in that a second pair of adjacent undulation of said structure is connected by means of a second connection element, in that in between said first and second pair of connection elements at least one undulation of an intermediate pair of undulations has an increased amplitude, to bridge at least part of the length of said first and second connection element. In this case the inevitable length of  
20 the connection elements between adjacent turns of the device is at least partly compensated by the increased amplitude of said at least one undulation, leading to a more uniform deployed stent-to-vessel ratio.

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Besides or even instead of being formed by a series of substantially helically staggered undulations, a substantially helically advancing pattern within the structure may also be created by the connection elements in themselves. <sup>In</sup> this respect, a specific embodiment of the endoprosthesis according to the invention is characterized in that said structure comprises at least one series of connection elements which are substantially regularly distributed over at least part of the length of said tubular body and in that successive  
30 connection elements within said at least one series are radially shifted to form one substantially helical pattern of said at least one substantially helical pattern within said



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embodiment

structure. More specifically, a preferred ~~embodiments~~ of the endoprosthesis according to the invention is characterized said successive connection elements are mutually connected by an elongated member which has a greater length than the linear distance between said connection elements in said first unexpanded state of the structure, in order to impart radial expandability to the structure.

In this manner a helically advancing spine is realised throughout at least a part of the device which adds to the scaffolding lattice of the structure, especially in the deployed state of the device. One or even more of such spines may give the device a considerable hoop-strength and supporting capability, without depriving the structure of its crimped as well as deployed flexibility. The greater length of the elongated member adds expandable diameter to the individually connected connection elements, imparting additional slack within the structure, an improved expandability and less fore-shortening on the device. This additional circumference allows for side branch access greater than the maximum expanded diameter of the stent along the longitudinal axis. In this respect, a specific embodiment of the endoprosthesis according to the invention is characterized in that said elongated member comprises a substantially S-curved bent. The S-curved members are situated along the spiral helix equidistantly spaced, along the longitudinal axis of the tubular body, and primarily allow the device to uniformly expand out radially enabling the structure to orient itself into a helical structure upon deployment. In a more particular embodiment the S-curved bent is orientated substantially parallel to the longitudinal axis of the tubular body, which allows the member to uniformly expand perpendicular to said axis. This prevents the device from twisting and rotating on the balloon-catheter, or the like, as the device undergoes expansion.

The endoprosthesis according to the invention may have a uniform structure throughout the device. A preferred embodiment of the device is however characterized in that the tubular body comprises a central portion, two outer portions at opposite ends of said tubular body and at least one intermediate portion in between the central portion and each of said end portions, the different portions being designed according to their

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specific function in the device. This embodiment is based on the recognition that different requirements may have to be imposed on different parts of the endoprosthesis to precisely meet the specific function or desired behaviour of the part concerned while the device is either unexpanded, expanded or in a transition between the unexpanded and expanded state. The present invention provides for a device in which this kind of tailoring may be implemented.

More particularly a further embodiment of the endoprosthesis according to the invention is characterized in that at least in one of the two outer portions of the tubular body the undulations in said structure have a gradually decreasing amplitude whether or not in combination with a changing pitch or filament width in order to render a free end of said portion substantially transverse to the longitudinal axis of said body, at least in said first unexpanded state of said structure. Such a square-like tubular end of the endoprosthesis prevents an undesired cantilever protrusion of the last turn which otherwise could harm the wall of the lumen while the device is being navigated to its intended position. Moreover this structure improves the mechanical bond between the endoprosthesis and the balloon of the catheter used to manipulate the device within the body. The square end is created by gradually decreasing the amplitude and changing the pitch of the last few undulations until there is a final smooth transition forming the desired square end. Modifications of the filament width at this area may further improve this part's behaviour.

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A still further embodiment of the endoprosthesis according to the invention is characterized in that said central portion of the tubular body comprises a first number of connection elements per full helical turn of said at least one substantially helical pattern within said structure, in that at least one of said intermediate portions comprises a second number of connection elements of the structure per full helical turn of said at least one substantially helical pattern within said structure, and in that the first number of connection elements is smaller than said second number of connection elements imparting a difference in flexibility between both portions of the tubular body. More precisely, the central portion will exhibit more flexibility than the intermediate portions

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due to the lower number of interconnections between adjacent turns. To accommodate this difference within the structure, a specific embodiment of the endoprosthesis according to the invention is characterized in that the central portion and anyone of said intermediate portions are separated from each other by a transitional portion in order to smoothly change the number of interconnections between adjacent turns from the first number to the second number of connection elements per full helical turn of said pattern.

Sub 108 In a more specific embodiment the endoprosthesis according to the invention is characterized in that adjacent turns in said central portion comprise a number of connection elements which are equally divided and in that connection elements in subsequent turns are helically shifted by approximately one undulation pitch distance. For example six adjoining helical segments with three equally spaced connection elements, situated approximately 120° with respect to one another or six opposing helical segments with two equally spaced connection elements situated approximately 180° with respect to one another. This specific design yields the most flexible structure in the central region, both crimped and deployed. Once deployed, the structure will orient itself in line with the helical lattice structure which it forms, exhibiting three intertwining continuous lattice legs within the intermediate region and only two of those legs in the central region. The intermediate region will <sup>possess</sup> ~~posses~~ more stiffness in order to counteract the balloon expansion, known as the "dog bone effect", which causes the ends of the device to flare prematurely prior to the deployment of the central section and which results in an undo amount of foreshortening upon expansion. Moreover the intermediate regions serve as a relief between the end portions and the central region of the device.

Ins a<sup>3</sup> The present invention will now be further described in more detail with reference to the following figures in which like elements are provided with the same reference numerals.

Fig. 1 shows an isometric view of an embodiment of an expandable intraluminal endoprosthesis in accordance with the present invention;

Fig. 2 is a plan view of the endoprosthesis of figure 1;

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Fig. 3 shows alternative embodiments of interconnection elements to be in a device according to the invention;

Fig. 4 is an enlarged view of an end portion of the endoprosthesis of figure 1;

Fig. 5 shows an isometric view of a second embodiment of an expandable intraluminal endoprosthesis in accordance with the present invention;

Fig. 6 shows a plan view of the device of figure 5 in a unexpanded state; and

Fig. 7 is a plan view of the device of figure 5 in a expanded, deployed state.

The figures are drawn merely schematically and not to scale. More particularly some dimensions may be exaggerated to more clearly point out one or more aspects of the present invention. Like parts the drawings are indicated as much as possible by like reference signs.

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Figure 1 gives an isometric view of an expandable intraluminal endoprosthesis according to a specific embodiment of the present invention. The endoprosthesis, hereinafter briefly referred to as stent, comprises a tubular member 1 which has been separated out of a tubular body of a suitable bio-compatible material. As such for instance high grade stainless steel (SST), a nickel-titanium based alloy referred to as Nitinol (NiTi), several cobalt based alloys and a Niobium-Titanium (NbTi) based alloy qualify. In this case the latter material may be chosen because of its excellent mechanical strength, corrosion resistance and radiopaque fluoroscopic signature. In the first, unexpanded state shown, the tubular member 1 is drawn with a first diameter  $d$  which permits delivery of the member into a lumen of a body passageway, particularly a blood vessel. The member 1 is capable of acquiring a second, expanded and deformed diameter upon the application of a radially outwardly extending force from its interior, usually by means of a balloon-catheter. This second diameter is variable and dependent on the amount of force applied. Inevitably the member will show a certain amount of recoil which means that the device will retract more or less after the balloon has been evacuated. Accordingly the second diameter will be slightly smaller than the diameter to which the stent has been expanded. Nevertheless the tubular member may be expanded and deformed to expand the lumen of the body passageway to again assure an undisturbed flow through the lumen, like a blood vessel.

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The wall of the stent comprises a substantially continuous structure which in this example consists of a continuous filament which has been cut out from the tube wall in a substantially helical fashion with a width between about  $0.10$  and  $0.17$  mm. This may be done by means of laser cutting, electrochemical etching, electromechanical discharge or any other suitable technique preferably followed by a suitable surface treatment, like etching to deburr and or round off possible sharp edges. In this example a tubular body with an internal diameter of about 3.0 mm, a wall thickness of about 1.0 mm and a length of about 30 mm has been chosen as a starting material. However other dimensions are likewise feasible within the scope of the present invention. Particularly the length may be adapted to the diseased part of the lumen to be stented in order to avoid the necessity of separate stents to cover the total area. The filament-structure comprises a number of undulations 2 which are mutually staggered in helical pattern advancing around a central longitudinal axis  $1-1$  of the device. In order to retain a coherent body subsequent turns  $2A-2H$  of the filament are interconnected by means of one or more connection elements 31, 32 which are entirely integral with the undulations thereby connected as they are cut altogether from one and the same tubular body. To retain flexibility, both unexpanded as well as deployed, the number of connection elements per helical turn is less than the number of undulations in said turn. This is further elucidated in figure 2 which gives plan view of the device as if it were cut open. As emerges <sup>quite</sup> clearly from this figure, the connection elements 31 to subsequent turns are radially shifted by about half undulation pitch distance  $\frac{1}{2}L$  to form a helical pattern X-X, Y-Y. Once deployed, these patterns will expand to a helically turning spines which form a primary framework or scaffolding lattice of the deployed stent. This framework supports the vessel wall highly uniformly throughout the device and moreover is capable of withstanding substantial inwardly directed radial forces, which is referred to as its hoop strength.

The lower drawing part of figure 2 shows a part of a central modular portion of the device in which successive turns of the filament are interconnected by means of only two connection elements 31, which are shifted about  $180^\circ$  with respect to one another, while the upper part shows an end portion of the device together with an intermediate

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portion in which three equally spaced connection elements 31,32 interconnect adjacent undulations from successive turns of the filament with each other. As a result the parent scaffolding lattice of the deployed device will be composed of only one helically advancing spine within the central region and will comprise two helically revolving spines within the other regions. Although the latter provides less flexibility, it leads to an improved adhesion to the balloon-catheter by which the device is guided through the lumen and moreover counteracts a so called dog bone effect, which is a premature expansion at the tail ends of the device. The central portion of the device, i.e. the lower drawing part, on the other hand retains maximum flexibility and conformability due to the smaller number of interconnections between adjacent undulations within this segment.

In this example two kinds of connection element are used, denoted 31 and 32 respectively. Both types of connection elements feature a strut 3 which is S-shaped and diagonally interconnects opposite sides of adjacent undulation from successive turns of the filament in a helical direction different to that of the staggered undulations themselves, see also figure 3E. These struts will be referred to as major struts as they are part of the lattice spines described hereinbefore. The second type of interconnection element 32 moreover features a second, S-shaped diagonal 4 strut intersecting the first one, see also fig 3D. Due to this shape an interconnection element of the second kind 32 will first start to rotate around its central axis once the stent is being deployed with only a limited force being exerted axially in the diagonal 3 of the connection element. Only after the first diagonal 3 has become fully in line with the sides of the undulations it interconnects, it has to withstand the entire force axially. This incorporated slack and stress relief allows thinner strut width and filament width over the lattice legs which can be useful for decreasing the radio-opacity at this area as well as improves its unexpanded, crimped as well as deployed, expanded flexibility. Moreover the support area covered by a connection elements of this second kind will not decrease much upon deployment of the device. As a result a larger "scaffolding footprint" will remain after deployment compared to any of the other types of connection elements shown which all

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will stretch substantially upon deployment leaving only the thin major strut 3 as "scaffolding footprint".

Besides the types connection elements depicted in the drawing also other shapes are feasible, as the invention imposes hardly no limitation of the design of any part of the device including the shape of the interconnections used. Examples of other shapes which could advantageously be used in a device according to the invention are shown in figure 3A-3G. The connection elements of figures 3A-3C merely comprise a straight strut 3 connection adjacent undulations, whereas the main strut 3 of the connection elements shown in figure 3D-3F have a clearly S-curved shape. This shape introduces more slack and expandability in the structure. The longer this segment, the more slack and expandability there is in the structure and especially in the spinal ladder created by these connection elements in the eventual deployed device. A simple formula can be derived from the expanded state, defining the relative increase of the strut length and the effect it has on the expansion range of the device.

The major strut 3, i.e. the strut eventually forming part of the parent scaffold or framework of the device once it is deployed, is indicated in figure 3 by a dotted hatch. In a special embodiment this strut as well as the undulation sides which it interconnects are given a first filament width  $w_1$  sufficiently large to withstand the axial forces imposed thereon during expansion of the device, whilst the other undulation sides and if applicable the other strut of the connection element are given a second filament width  $w_2$ , at least locally, to gain flexibility and decrease radio-opacity. Specifically the filament width is modified in the central portion of the device to improve its overall flexibility such that a first filament width  $w_1$  of approximately  $0.14$  mm is taken whereas the second filament width  $w_2$  is reduced to about  $0.11$  mm.

In order to avoid a substantial disruption of the stent to vessel support by pairs of undulations from successive turns of the filament which are not mutually interconnected by a connection element, the amplitudes of the undulations within such pair may be adapted to fill the gap which would otherwise remain due to the inevitable length of a

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connection element elsewhere in the structure. This is for instance apparent from figure 2 where all adjacent peaks and valleys of pairs of undulations out of successive turns which are not interconnected nevertheless adjoin one another. This is a result of the adapting the amplitude of at least one of the undulations within such pair of undulations.

5 This can imply that both, the peak and the valley have an increased amplitude, that only one of those parts is enlarged, the other part remaining unchanged, or even that either the peak or the valley has a increased amplitude while the other part has a decreased amplitude. Also in this respect, the designer has full freedom to tailor the stent design to allow optimal behaviour of the stent in its unexpanded state, expanded and/or  
10 transitional state.

The end portion of the device ends substantially transverse to the central axis of the device in order to avoid a cantilever usually associated with a helix shape which could otherwise harm the wall of the lumen through which the stent is navigated. This end  
15 portion is shown in more detail in figure 4. Its particular shape is obtained by gradually decreasing the amplitude in the last few undulations and adapting their mutual pitch. Due to the invention this may be done without introducing any stress in the device as the filament is simply cut in the desired pattern. The deviating amplitudes and mutual pitch are best recognized from the plan view of figure 2. The end modules exhibit a greater  
20 stent-to-vessel ratio than the central and intermediate portions due to the increased metal-to-surface-area in the expanded configuration. The more complex structure of the end portions moreover give rise to a greater amount of foreshortening upon expansion, thus producing a more dense pattern yielding additional stent-to-vessel ratio.

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A second embodiment of the device according to the invention is depicted in figures 5-  
7. This device comprises a tubular body 1 and has been manufactured using similar  
techniques as the first embodiment, although in this case a more complicated structure  
has been created consisting of more than just a single, wrapped filament. However, like  
in the first embodiment, the structure of the device is composed of a substantially helical  
30 pattern of mutually staggered undulations 2, with connection elements 33  
interconnection some undulations from successive turns of said pattern. The connection





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Although the invention has been described hereinbefore with reference to merely a few embodiments, it will be appreciated that the invention is far more wide spread applicable. Within the scope of the invention many other embodiments and variations are feasible for a skilled practitioner. As such he may vary for instance the mutual pitch of a few or more subsequent undulation with or without a variation of the amplitude in order to tailor the stent-to-vessel ratio and flexibility at the area concerned. Also, additional modular portions individually recognizable in the stent could be implemented in the stent in order to add specific functionality. As such, a transitional portion might be interposed between the relatively flexible central portion and the more stiff intermediate and end portion in order to alleviate the structural transition between those parts of the stent. Also the number of connection elements within a full turn of the helical pattern may be raised to introduce additional lattice spines to the deployed device, resulting in even a larger hoop strength and supporting capability of the device.

Likewise, the filament width as well as undulation shapes may be varied and adapted to suit specific required characteristics besides the flexibility and stent-to-vessel ratio. For instance, the foreshortening of the device, i.e. the amount of length reduction upon expansion from the crimped to the deployed state of the device, its degree of recoil, its hoop strength as well as its radio-opacity. In any event the present invention provides the designer with the greatest amount of freedom conceivable.

Also the elongated members interlinking a series of connections <sup>elements</sup> like in the second embodiment need not coincide with undulations of the pattern and can be introduced in the structure as separate elements. These members moreover need not necessarily comprise a full S-curved bent or even no S-curved bent at all and may on the other hand consist of more than just one such bent. Also in this respect the designer has total freedom to tailor the device to his demands.